



HAL
open science

Experimental study of a liquid Xenon PET prototype module

M.-L. Gallin-Martel, P. Martin, F. Mayet, J. Ballon, G. Barbier, C. Barnoux, J. Berger, D. Bondoux, O. Bourrion, J. Collot, et al.

► **To cite this version:**

M.-L. Gallin-Martel, P. Martin, F. Mayet, J. Ballon, G. Barbier, et al.. Experimental study of a liquid Xenon PET prototype module. 7th International Workshop on Radiation Imaging Detectors (IWORID-7), Jul 2005, Grenoble, France. in2p3-00024907v1

HAL Id: in2p3-00024907

<https://in2p3.hal.science/in2p3-00024907v1>

Submitted on 7 Nov 2005 (v1), last revised 23 Nov 2005 (v2)

HAL is a multi-disciplinary open access archive for the deposit and dissemination of scientific research documents, whether they are published or not. The documents may come from teaching and research institutions in France or abroad, or from public or private research centers.

L'archive ouverte pluridisciplinaire **HAL**, est destinée au dépôt et à la diffusion de documents scientifiques de niveau recherche, publiés ou non, émanant des établissements d'enseignement et de recherche français ou étrangers, des laboratoires publics ou privés.

Experimental study of a liquid Xenon PET prototype module

M.-L. Gallin-Martel¹, P. Martin, F. Mayet, J. Ballon,
G. Barbier, C. Barnoux, J. Berger, D. Bondoux, O. Bourrion,
J. Collot, D. Dzahini, R. Foglio, L. Gallin-Martel, A. Garrigue,
S. Jan², P. Petit, P. Stassi, F. Vezzu, E. Tournefier³

*Laboratoire de Physique Subatomique et de Cosmologie, CNRS/IN2P3 et
Université Joseph Fourier, 53, avenue des Martyrs, F-38026 Grenoble cedex,
France*

*submitted to Proc. of the 7th International Workshops on Radiation Imaging
Detectors, 4-7 july 2005, Grenoble, France*

Abstract

A detector using liquid Xenon in the scintillation mode is studied for Positron Emission Tomography (PET). The specific design aims at taking full advantage of the liquid Xenon properties. It does feature a promising insensitive to any parallax effect. This work reports on the performances of the first LXe prototype module, equipped with a position sensitive PMT operating in the VUV range (178 nm).

Key words: Positron emission tomography (PET), Medical imaging equipment
PACS : 87.58.Fg ; 87.62.+n

1 Introduction

Positron Emission Tomography (PET) is one of the leading techniques of nuclear medicine to access to metabolic and functional information. PET is used

¹ Corresponding author : Tel.: +33-476-284-128; fax: +33-476-284-004; e-mail: ml-gallin@lpsc.in2p3.fr.)

² Present address : Service Hospitalier Frédéric Joliot (SHFJ), CEA, F-91401 Orsay, France

³ Present address : Laboratoire d'Annecy-le-Vieux de Physique des Particules, CNRS/IN2P3, BP 110, F-74941 Annecy-le-Vieux cedex, France

for various medical and biological applications, such as oncology, cardiology as well as pharmacology. Experimental efforts on a host of techniques have been made in the field of PET imaging, in particular towards the development of new generation high resolution PET cameras dedicated to small animal imaging [1,2,3]. A couple of years ago, we proposed to use liquid Xenon in an axial geometry for a scintillation based PET [4,5,6]. This paper presents the experimental results on the first LXe prototype module, in terms of spatial resolution in the axial and transaxial coordinates.

2 The geometry of the Liquid Xenon PET camera

The active part of this project of LXe camera is a ring featuring an internal diameter of 8 cm and a radial extension of approximately 25 mm (see Fig. 1). It is filled with liquid Xenon and placed in a cryostat composed of thin aluminum walls. Sixteen identical modules of the type shown on Fig. 2, are immersed in this ring. Each module presents a 2×2 cm² cross-section in the transaxial plane of the camera. The axial field of view is 5 cm. A module is optically subdivided by one hundred 2×2 mm² MgF₂-coated aluminum UV light guides. The UV light is collected on both sides of a module by two Position Sensitive PhotoMultiplier Tubes (PSPMT). The (x,y) positions measured by the photo-tubes determine which light guides have been fired. For each module, the axial coordinate is provided by the following ratio of the photo-tube signals :

$$Z = (PMT_1 - PMT_2)/(PMT_1 + PMT_2)$$

allowing to measure the transaxial Depth Of Interaction (DOI) of the photons.

3 Experimental set-up

Following the layout displayed on Fig. 3, the Xenon is liquefied in a first container called the compressor, then transferred to a container inside the cryostat. The temperature inside the cryostat is kept around 165 K via a liquid nitrogen heat exchanger. The temperature is constant to better than a few tenths of a degree. The Xenon container is a stainless steel cylinder 50 mm long and 40 mm in diameter, closed at each end with a suprasil 3 mm thick window. A ²²Na source is mounted on a small carriage moving along the z direction. A LYSO crystal coupled to a photomultiplier tube completes the experimental set-up to make the coincidence signal. The VUV photons are then collected with one PSPMT at each end. PSPMT with the required

specifications, high Quantum Efficiency (QE) at 178 nm, and still working at low temperatures (165 K), cannot be taken from the shelf yet. Hamamatsu provided us with two prototype tubes, from the R8520-06-C12 series [7], having five aluminum strips deposited on their window to improve the resistivity of the photocathode at 165 K. QE was around 20% but the resistivity was still rather high.

The read out electronics operates at room temperature and is composed of standard NIM and CAMAC modules. The acquisition software performs barycentre online calculation.

4 Experimental results

4.1 PSMPT spatial resolution and x and y localization

To evaluate the PSPMT spatial resolution, a deuterium light source is used to produce a constant number of photons in a wide wavelength range. To level down the number of photons emitted, dedicated light attenuators are placed in front of the light source. Then to focus the light pulse on a specific area defined on the PSPMT surface, the light emitted by the source is collected via an optical fibre going through an opaque plastic disk placed in front of the PSPMT window. This disk exhibits a matrix of holes equally spaced. The number of photoelectrons is derived from the dynode signal distribution. The x and y barycentre distributions is computed on-line by the DAQ and derived of the anode signals. The resolution in x and y as a function of the number of photoelectrons (N_{pe}) is illustrated by Fig. 4. The resolution is increasing with N_{pe} , ranging from 0.32 mm down to 0.18 mm for $N_{pe} = 300$. This experimental study concludes that the PSPMT spatial resolution is fine for our application. The resolution is at the level of 1 mm in the x and y directions which is in very good agreement with the simulation [8]. The second step of this analysis was to study the light guide separation in the transaxial plane. It has been evaluated using an ^{241}Am α source located at one end of the Xenon container. The advantage of using an α source in the liquid is to give intense point-like sources of photons, at a well defined distance of the PSPMT. Three different matrix of light guides were used for the tests, with cross sections of 2×2 , 5×5 and 2×5 mm², within an overall cross section of 20×20 mm². In the 2×5 configuration, the module had therefore only 40 cells of 48 mm in length. The walls of these cells are made of a double 35 μm thick aluminum foil, double because specular reflection has been guaranteed on one side only : the basic material is a 35 μm aluminum foil, with a thin polyethylene film glued on one side to reduce the crookedness of its surface, followed with evaporation of

aluminum again and MgF_2 to make the actual reflecting surface. The Fig. 5 obtained with a guide matrix of $2 \times 5 \text{ mm}^2$ shows a very satisfying light guides separation in the (x,y) transverse plane.

4.2 Localization and resolution along the z axis

The specific design of the liquid Xenon PET prototype employs the Depth Of Interaction (DOI) approach to solve the problem of parallax errors. It permits a continuous measurement of the z coordinate. An experimental test bench (see section 3 and Fig. 3) has been built to measure the module prototype resolution in Z. The Z coordinate is deduced from the amplitude of the dynode signals measured on the right and left PSPMT located at each side of the module, as defined in section 3.

The resolution at a z position will be given by the FWHM of the obtained distributions. The resolution as a function of the source localization is illustrated by Fig. 6. The resolution is better at the module extremities rather than at the central position where it is about 10 mm. This result is not as good as expected but a refined simulation of the light collection in optical guides has been done and three configuration for the light collection units (present setup with the PSPMT, PSPMT immersed in the LXe, windowless APD immersed in the LXe) have been compared [8], this analysis concludes that a higher resolution can be achieved by :

- increasing the reflectivity of the light guide using other manufacturing processes (the current value for the reflectivity is 0.78),
- immersing the PSPMT in the liquid or by using high quantum efficiency Avalanche Photodiodes this is under way.

5 Conclusion

First test of a liquid Xenon TEP prototype module were carried out. The preliminary results of the experimental study allow us to determine the intrinsic performance of this camera. The localization in the transaxial plane is very satisfying : the resolution is better than 0.3 mm in the x and y directions. Efforts are to be made for the localization in the axial direction since the resolution in z is not only position dependent of the γ source used for the test but exhibits a poor average value of about 8 mm. Simulation of the light collection in optical guides and in various light collection units (PSPMT at the LXe temperature but not immersed in the liquid, PSPMT immersed in the LXe, windowless APD immersed in the LXe) concludes that a higher

resolution can be achieved [8]. Two next steps are foreseen. At first, the light guide reflectivity (currently 0.78) is to be improved, a new process is under study. Then the VUV light collection on each module end would be better by using high quantum efficiency windowless APD. We aim to investigate now these two possibilities.

Acknowledgments :

This work has been made possible thanks to the financial grants allocated by the Rhône-Alpes region through its “Emergence” science program, and by the CNRS/INSERM via its IPA program dedicated to the small animal imaging. We are also indebted to Jean-François Le Bas and Daniel Fagret of the medical department of the Joseph Fourier University of Grenoble for the support and motivation they brought to this project. We also wish to thank the technical staff of LPSC and in particular : Y. Carcagno, P. Cavalli, E. Lagorio, G. Mondin, A. Patti and E. Perbet.

References

- [1] S. Weber and A. Bauer, European Journal of Nuclear Medicine and Molecular Imaging 2004, *in press*
- [2] Y. Yang *et al.*, Phys. Med. Biol. **49** (2004) 2527
- [3] K. Wienhard *et al.*, IEEE Trans. Nucl. Sci. **49** (2001) 104
- [4] J. Collot *et al.*, Proc. of the IXth Intern. Conference on Calorimetry in High Energy Physics (CALOR 2000), Oct. 2000, Annecy (France), Eds. B. Aubert *et al.* (Frascati Physics Series Vol 21), pp. 305
- [5] S. Jan *et al.*, *to appear in* Proc. of International Conference Imaging Technologies in Biomedical Sciences (ITBS 2001), May 2001, Milos Island (Greece)
- [6] S. Jan, PhD Thesis, Université Joseph Fourier (Grenoble, France), Sept. 2002
- [7] Hamamatsu Photonics, 8 Rue du Saule Trapu, Parc du Moulin de Massy, 91300 Massy, France
- [8] M-L Gallin-Martel *et al.*, *A liquid Xenon PET : prototype cell results*, to be submitted to Nucl. Instr.and Meth.

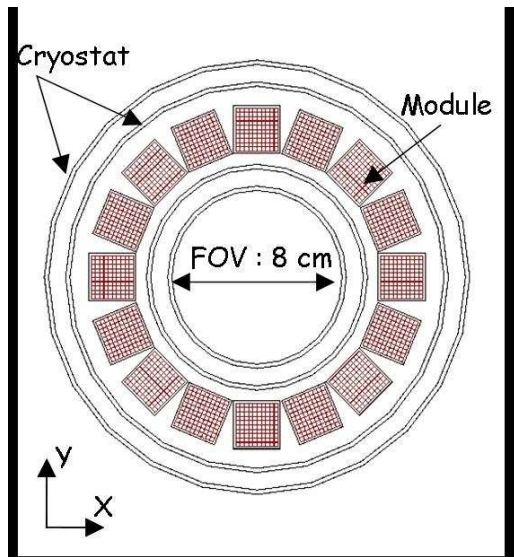


Fig. 1. Transaxial view of the LXe μ PET

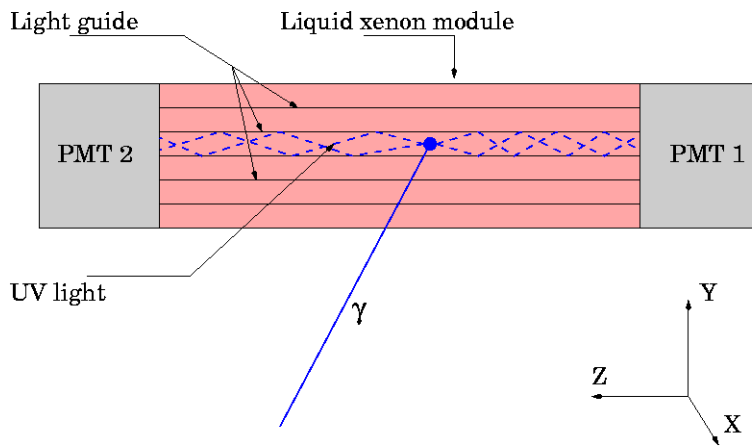


Fig. 2. Sketch of an elementary module of the LXe μ PET camera : the z -axis is along the axial direction of the μ PET.

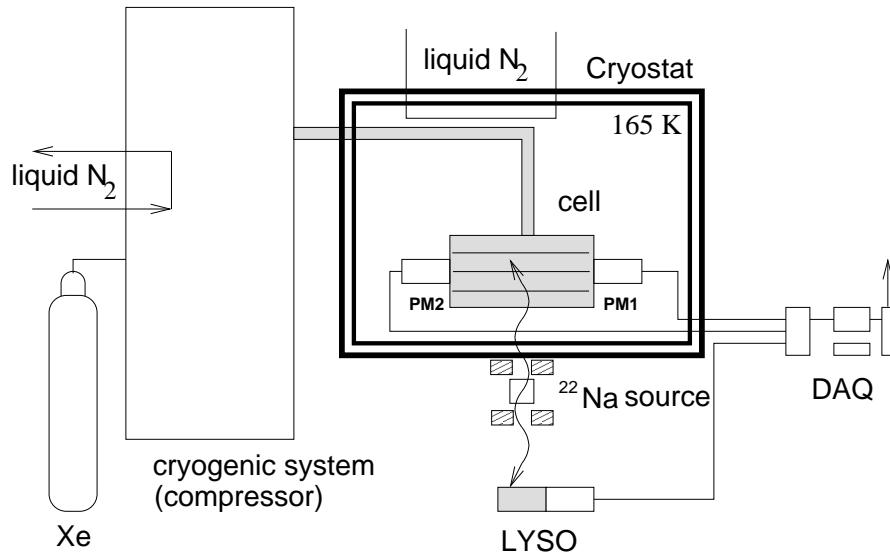


Fig. 3. Experimental set-up used for the test of the prototype module.

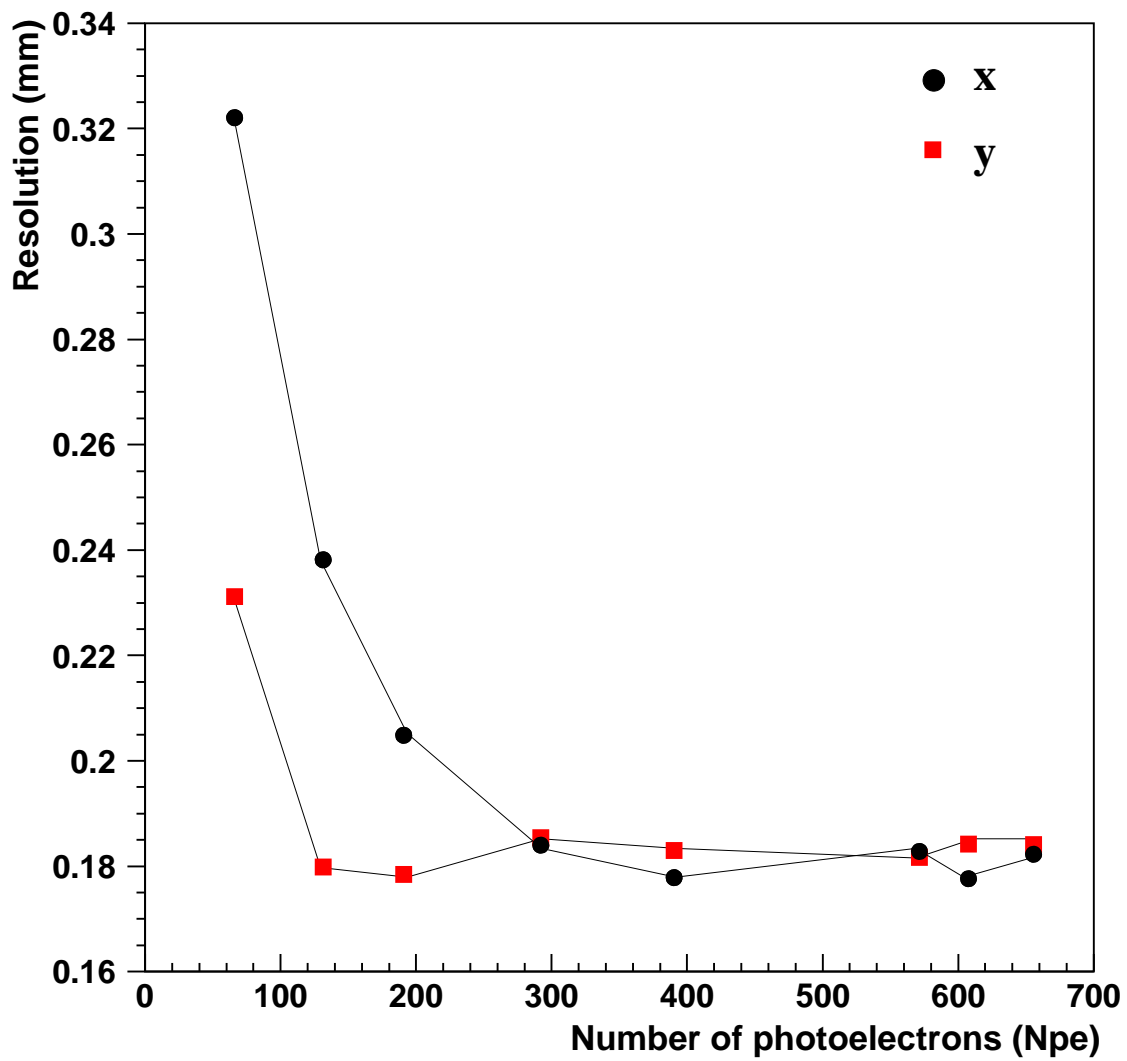


Fig. 4. The resolution in X and Y as a function of the number of photoelectrons.

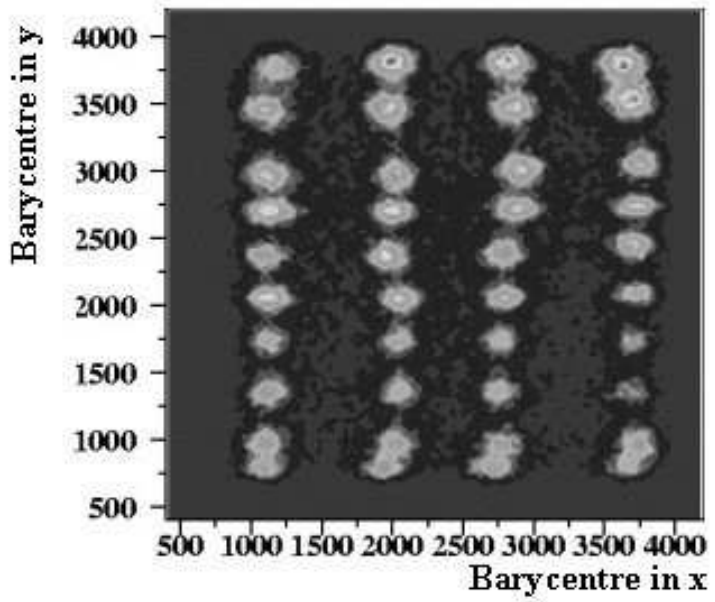


Fig. 5. X and Y localization using the $2 \times 5 \text{ mm}^2$ light guides configuration.

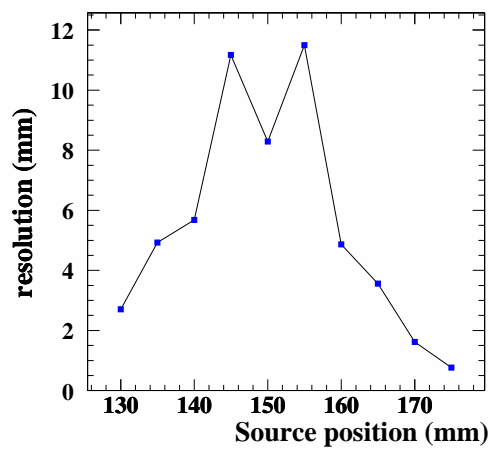


Fig. 6. Axial resolution as a function of the source localization